


VERDICT prostate parameter estimation with AMICO

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Abstract. The VERDICT (Vascular, Extracellular and Restricted Diffusion for Cytometry in Tumours) technique estimates non-invasively cancer microstructure features. The clinical application of VERDICT for prostate cancer requires constraining some of the models parameter. This work uses the Accelerated Microstructure Imaging via Convex Optimization (AMICO) formulation for VERDICT (VERDICT-AMICO), to investigate parameter estimation for prostate tissue, in an attempt to minimize the parameter constraints. We examine various dictionaries for VERDICT-AMICO enabling different levels of flexibility on the choice of parameter values. Depending on the stability of the fitting this procedure leads to the selection of a dictionary (or dictionaries) with the fewest number of model parameter constraints. Results show that with the current VERDICT imaging acquisition, the model can have an extra free parameter to fit, the extracellular diffusivity. In conclusion, the AMICO adaptation for VERDICT allowed testing of different values for the previously fixed model parameters, and helped relax assumptions of fixed extracellular diffusivity that the model currently uses for prostate cancer characterisation.

Keywords: VERDICT-AMICO, microstructure characterisation, prostate cancer

1 Introduction

Prostate cancer is the most common cancer among men in all economically developed countries[1]. A non-invasive method of diagnosis and grading would revolutionise clinical practice. The VERDICT (Vascular, Extracellular, and Restricted

Diffusion for Cytometry in Tumours) model [2, 3] is a three compartment model-based technique that is designed to capture the main microstructural properties of cancerous tissue. VERDICT has shown promising results in preclinical studies for characterising microstructural tissue properties of xenograft tumour models [3] and in a pilot clinical setting for discriminating benign and malignant prostate tissue [2]. Currently, VERDICT is being tested as part of the INNOVATE clinical trial [4] for prostate cancer characterisation. Diffusion-weighted MRI (DW-MRI) is becoming increasingly important in the assessment of malignant tumours [5]. Model-based quantitative imaging techniques like VERDICT can ameliorate problems with simplistic diffusion-based indices, such as Apparent Diffusion Coefficient (ADC), by estimating parameters reflecting separate biophysical influences on the signal. However, the original implementation of VERDICT requires a computationally expensive non-linear fitting procedure to estimate the model parameters, which limits its use in large cohort studies and real-time clinical applications. Ultrafast fitting algorithms, such as the Accelerated Microstructure Imaging via Convex Optimization (AMICO) framework [6], have been developed to address the computational cost of model-based microstructure-imaging techniques.

The first implementation of the AMICO formulation for the VERDICT model (VERDICT-AMICO) in prostate tissue [7] performed a direct comparison of non-linear fitting and AMICO fitting for the VERDICT signal model and parameter constraints used in [2]. VERDICT-AMICO showed a good agreement with the non-linear VERDICT fitting. Parameter maps obtained revealed qualitatively similar differences between tumour and normal tissue. Furthermore, VERDICT-AMICO computes the estimates for tissue microstructure faster than the previous non-linear fitting technique and locates the global minimum parameter values more reliably. However, VERDICT-AMICO inherits some parameter constraints from the original non-linear implementation, which could be relaxed due to the enhanced stability of the AMICO fitting.

Here, we aim to find a stable implementation for the VERDICT model that imposes the least constraints on the parameters values. Thus, we use AMICO to fit the VERDICT model for prostate cancer as published previously [7] and to explore the possibility of unfixing previously fixed model parameters by trying various dictionaries for VERDICT-AMICO. Specifically, we investigate which parameters should remain fixed due to lack of sensitivity intrinsic in the data (i.e. number of acquisitions), and which constraints can be relaxed to increase biological realism. This improves the quantitative nature of the maps we obtain; we also consider retaining qualitative conspicuity for the original parametric maps in the cancer lesion areas, which are clinically important.

2 Material and Methods

This section describes the VERDICT model and VERDICT-AMICO [7], the direct adaptation of VERDICT model for prostate [2] using the AMICO framework [6]. We also provide details of the MRI acquisition and the patient population.

2.1 VERDICT

The VERDICT model characterizes water diffusion in three different compartments in tumours: vascular (VASC), extracellular-extravascular (EES), and intracellular (IC). Mathematically, VERDICT is the addition of three parametric models without considering exchange between them. The normalized diffusion signal for the VERDICT model is:

$$S = \sum_{i=1}^3 f_i S_i \quad (1)$$

where f_i is the proportion of signal with no diffusion weighting ($b=0$) from water molecules in population i (VASC, EES or IC), $0 \leq f_i \leq 1$, $\sum_{i=1}^3 f_i = 1$.

In the VERDICT model for prostate cancer in [2] the diffusion signal for the intracellular (IC) compartment is modelled with impermeable spheres and has (IC diffusivity) and (cell radius) as parameters. The model for the extracellular-extravascular space (EES) compartment is an isotropic diffusion tensor with (diffusivity EES) as parameters. The vascular compartment uses the ‘‘Astrostick’’ model (using the terminology of [8] for isotropically distributed negligibly-thin restricting cylinders) and has (pseudo-diffusivity) as parameters. The clinical implementation of the VERDICT model has only 3 independent unfixed parameters: f_{IC} , R and f_{EES} . The vascular volume fraction was calculated as $f_{VASC} = 1 - f_{IC} - f_{EES}$, and the diffusion and pseudo-diffusion coefficients were fixed to $d_{IC} = d_{EES} = 2 \times 10^{-9} \text{ m}^2/\text{s}$, $P = 8 \times 10^{-9} \text{ m}^2/\text{s}$ [2].

2.2 VERDICT-AMICO

Accelerated Microstructure Imaging via Convex Optimization (AMICO) have been developed to address the computational cost of model-based microstructure-imaging techniques [6]. AMICO linearises the fitting problem using a dictionary composed with synthetic signals simulating the number of measurements per voxel (N_d).

In the first implementation of VERDICT-AMICO, the dictionary $\Phi = \{\phi_{ij}\} \in \mathbb{R}_+^{N_d \times N_k}$ was partitioned in three sub-matrices corresponding to the three VERDICT compartments:

$$\Phi = [\Phi^r | \Phi^e | \Phi^v] \quad (2)$$

where $\Phi^r \in \mathbb{R}^{N_d \times N_r}$, $\Phi^e \in \mathbb{R}^{N_d \times N_e}$ and $\Phi^v \in \mathbb{R}^{N_d \times N_v}$ model the IC, EES and vascular contributions of the diffusion signal in the voxel with $N_k = N_r + N_e + N_v$. The regularization function used is the basic Tikhonov regularization with the same λ value ($\lambda = 0.001$) used in [7] that was set empirically. The full dictionary consists of $N_k = 19$ entries in total combining three sub-dictionaries as follows:

- Each column in $\Phi^r \in \mathbb{R}^{N_d \times N_r}$ corresponds to the signal attenuation of the water molecules restricted within spheres with a specific radius. $N_r = 17$

different radii values linearly spaced from 0.01 to 15.1 μ m (both values included). The corresponding signal profiles are estimated according to the sphere model (using the name from [8]), assuming $d_{IC} = 2 \times 10^{-9} m^2/s$.

- A single compartment, $\Phi^e \in \mathbb{R}^{N_d \times N_e}$ where $N_e = 1$ describes the EES with the same fixed value for the diffusion coefficient $d_{EES} = 2 \times 10^{-9} m^2/s$. Signal is estimated according to the ball model (terminology in [8]).
- A single compartment, $\Phi^v \in \mathbb{R}^{N_d \times N_v}$ where $N_v = 1$ is considered to account for the vascular volume fraction. Signal is estimated according to the “Astrostick” model and pseudo-diffusivity (perfusion) is fixed $P = 8 \times 10^{-9} m^2/s$.

2.3 Patients and Data Acquisition and Processing

This study was performed with local ethics committee approval as part as the INNOVATE clinical trial [4]. Between April and June 2016, 6 men were prospectively recruited and provided informed written consent. The inclusion criteria for these patients were (1) suspected prostate cancer or (2) undergoing active surveillance for known prostate cancer. Exclusion criteria were: (1) previous hormonal, radiation therapy or surgical treatment for prostate cancer and (2) biopsy within 6 months prior to the scan.

All patients underwent a standard multi-parametric prostate (mp)-MRI [9], on a 3T scanner (Achieva, Philips Healthcare, NL) supplemented by VERDICT DW-MRI. VERDICT DW-MRI was acquired using a pulse-gradient spin-echo sequence and an optimized imaging protocol for prostate adapted from [10] with five b values between 90-3000s/mm in 3 orthogonal directions. Table 1 summarises the Δ , δ , $|G|$, TE and TR corresponding to each b-value. VERDICT-MRI data was registered using a rigid registration [11, 12] and then normalised with the b=0 image for every TE to avoid T2 dependence. The number of normalized measurements per voxel is $N_d = 20$.

Table 1. Optimized imaging protocol for VERDICT prostate characterisation. Δ is the gradient separation time, δ is the gradient duration, $|G|$ is the gradient strength, TE is the echo time and TR is the repetition time.

b-values [s/mm]	Δ [ms]	δ [ms]	$ G $ [ms]	TE[ms]	TR[ms]
90	23.8	3.9	61.2	50	2482
500	31.3	11.4	44.3	65	2482
1500	43.8	23.9	32.0	90	2482
2000	34.3	14.4	67.7	71	3945
3000	38.8	18.9	60.0	80	3945

MR datasets were visualized with Osirix Version 7.0 (Bernex, Switzerland). For each subject a board-certified radiologist (EJ) manually contoured (Osirix 7.0) different regions of interest (ROIs) in the VERDICT-AMICO maps corresponding to tumour and normal tissues in transition zone (TZ) and peripheral

zone (PZ). The total number of ROIs was 20. To examine similar histological areas, we grouped the ROIs according to tumour grading and the prostate zone, which resulted in 10 different ROI groups (g-ROI) with homogeneous tissue.

3 Experiments and Results - Parameter Fitting

The first experiments (3.1) explore the free VERDICT model using AMICO with a wide range of parameters values. Subsequent experiments (3.2-3.3) explore which parameters can be fixed to ensure fitting stability, while retaining an extensive dictionary for the unfixed parameters. The different dictionaries used are summarised in Table 2.

3.1 Unfixed model

The VERDICT model fitting in prostate requires fixed parameters to achieve stable estimates [2]. This experiment uses the free tissue model to investigate the range of the parameter estimates with VERDICT-AMICO. The number of measurements limits the dictionary size for the VERDICT-AMICO implementation and this restricts the values for the selected ranges in each sub-matrix. Accordingly, we use four different dictionaries for fixing different pseudo-diffusivity P values in each while unfixing d_{IC} and d_{EES} . We retain the following constraints for physical realism: $1 \times 10^{-11} m^2/s \leq d_{IC} \leq 2.9 \times 10^{-9} m^2/s$, $d_{IC} = d_{EES}$ and $3 \times 10^{-9} m^2/s \leq P \leq 9 \times 10^{-8} m^2/s$. The full dictionaries for VERDICT-AMICO consist of $N_k = 19$ entries, as follows:

- $N_r = 15$ combinations of 5 different radii (linearly spaced from 0.01 to $15.1 \mu m$) and 3 different d_{IC} (1.2×10^{-9} , 1.7×10^{-9} and $2.1 \times 10^{-9} m^2/s$).
- $N_e = 3$ describes the EES with the same fixed value for the diffusion coefficient $d_{EES} = 1.2 \times 10^{-9}$, 1.7×10^{-9} and $2.1 \times 10^{-9} m^2/s$.
- $N_v = 1$, was fixed for each dictionary. The four different values are: (1) $P = 3 \times 10^{-9} m^2/s$, (2) $P = 1 \times 10^{-8} m^2/s$, (3) $P = 3 \times 10^{-8} m^2/s$ and (4) $P = 6 \times 10^{-8} m^2/s$. Signal is estimated according to the ‘‘Astrostick’’ model in [8].

Fig. 1 shows that VERDICT-AMICO performance for the new dictionaries (with unfixed d_{IC} and d_{EES} parameters) is unstable for most parameters and especially for R , f_{VASC} and f_{EES} where the estimates present high variations depending on the dictionary. The parameter values obtained with the original dictionary (fixed values for P , d_{IC} and d_{EES}) are also shown as reference. Results also reveal a trend (values are not fluctuating randomly) in the values of the perfusion coefficient P (or pseudo-diffusivity), allowing us to identify a value and fix this parameter.

3.2 Fixing Parameters - Perfusion

Since values show little variation, here we examine different pairings of and to find at which value the should be fixed, as different d_{IC} values had only a minor

Table 2. Summary of the dictionaries to show which parameter is fixed and its value. Values in bold are unfixed. d_{IC} and d_{EES} values are multiplied by 10^{-9} if not stated differently.

Model/Experiment	f_{IC}	d_{IC} [m^2/s]	R [μm]	f_{EES}	d_{EES} [m^2/s]	f_{VASC}	P [m^2/s]
VERDICT[2]	0-1	2	0.01-15	0-1	2	$1 - f_{IC} - f_{EES}$	$8x10^{-9}$
VERDICT-AMICO[7]	0-1	2	0.01-15.1	0-1	2	0-1	$8x10^{-9}$
Experiment 3.1 (unfixed models)	0-1	1.2-2.1	0.01-15.1	0-1	1.2-2.1	0-1	$3x10^{-9}$ $1x10^{-8}$ $3x10^{-8}$ $6x10^{-8}$
Experiment 3.2 (fixed d_{IC} - P pairs)	0-1	{1.0, 1.2, 1.5, 1.8, 2.0, 2.1, 2.3, 2.6, 2.8, 3.1}	0.01-15.1	0-1	1.1-3.1	0-1	{ $8x10^{-9}$, $1x10^{-8}$, $3x10^{-8}$, $6x10^{-8}$, $1x10^{-7}$ }
Experiment 3.3	0-1	{ $8x10^{-10}$, 1.0, 1.2, 1.4, 1.5, 1.6, 1.8, 2.0, 2.1, 2.2, 2.3, 2.6, 2.8, 2.9, 3.1}	0.01-15.1	0-1	1.1-3.1	0-1	$8x10^{-9}$
VERDICT-AMICO (unfixed d_{EES})	0-1	2	0.01-15.1	0-1	1.1-3.1	0-1	$8x10^{-9}$

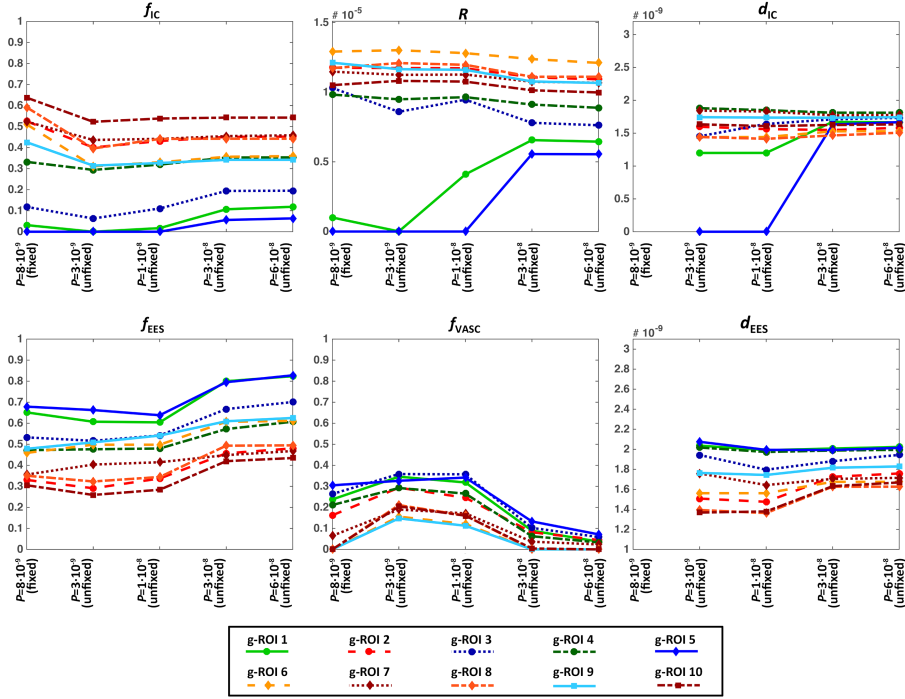


Fig. 1. Parameter estimates for all voxels within each of the grouped-ROIs (g-ROI), median values represented. First measures correspond to $P = 8 \times 10^{-9} m^2/s$ with fixed values for d_{IC} and d_{EES} . The other points correspond to estimated values using the dictionary with unfixed d_{IC} and d_{EES} for different fixed perfusion values. R in $[\mu m]$.

effect on the fitting. This is also supported by [13], where the study finds minimal effects from fixing the intracellular diffusivity.

In this work, fixing d_{IC} and P allows us (i) to increase the range of radii values in the dictionary, which could potentially enable capturing a greater range of cell types with different cell sizes, and (ii) to increment the range of d_{EES} values, which could be useful for detecting different EES tissue features (e.g. to better characterize lumen and large stromal cells).

To fix P we first test 50 different $d_{IC} - P$ fixed pairs using the following dictionary for the rest of the parameters:

- $N_r = 13$ different radii (linearly spaced from 0.01 to $15.1\mu\text{m}$).
- $N_e = 5$ diffusion coefficient for EES. $d_{EES} = 1.1 \times 10^{-9}$, 1.6×10^{-9} , 2.1×10^{-9} , 2.6×10^{-9} and $3.1 \times 10^{-9} \text{m}^2/\text{s}$.
- $N_v = 1$, fixed for each dictionary.

The fixed values for the $d_{IC} - P$ combinations are:

- 5 values for perfusion: $P = 8 \times 10^{-9} \text{m}^2/\text{s}$, $P = 1 \times 10^{-8} \text{m}^2/\text{s}$, $P = 3 \times 10^{-8} \text{m}^2/\text{s}$, $P = 6 \times 10^{-8} \text{m}^2/\text{s}$ and $P = 1 \times 10^{-7} \text{m}^2/\text{s}$.
- 10 values for intracellular diffusivity: $d_{IC} = 1.0 \times 10^{-9}$, 1.2×10^{-9} , 1.5×10^{-9} , 1.8×10^{-9} , 2.0×10^{-9} , 2.1×10^{-9} , 2.3×10^{-9} , 2.6×10^{-9} , 2.8×10^{-9} and $3.1 \times 10^{-9} \text{m}^2/\text{s}$.

We compute the median value for each parameter for all voxels within each of the grouped-ROIs for each $d_{IC} - P$ pair. Most of the estimates plateau or present minor variations for all the values (with fixed intracellular diffusivity) for the majority of both ROIs and g-ROIs. This trend can be qualitatively observed in the f_{IC} maps for two different patients in Fig.2.

The radiologist EJ examined the VERDICT maps for tumour conspicuity to ensure tumour enhancement and clinical relevance. In general, all maps appear similar for different perfusion coefficients with small variations revealed by the objective function. As in previous results (see Fig. 1) the perfusion value used for the dictionary has minor effect on the fitting. Thus, we fix perfusion to the original value $P = 8 \times 10^{-9} \text{m}^2/\text{s}$ without compromising qualitative tumour conspicuity.

3.3 Fixing Parameters - Intracellular Diffusivity

To identify the best value to fix the intracellular diffusivity parameter we fix perfusion at the original value and repeat the same experiment increasing the number of values for d_{IC} . We test 15 values for intracellular diffusivity: $d_{IC} = 8.0 \times 10^{-10}$, 1.0×10^{-9} , 1.2×10^{-9} , 1.4×10^{-9} , 1.5×10^{-9} , 1.6×10^{-9} , 1.8×10^{-9} , 2.0×10^{-9} , 2.1×10^{-9} , 2.2×10^{-9} , 2.3×10^{-9} , 2.6×10^{-9} , 2.8×10^{-9} , 2.9×10^{-9} and $3.1 \times 10^{-9} \text{m}^2/\text{s}$.

Fig. 3 shows the median value for each d_{IC} value for the g-ROIs, each represented in different colours. Most of the estimates, including the objective function, present small variations within the varying intracellular diffusivity as in [13], so we fix the diffusivity at $d_{IC} = 2.0 \times 10^{-9} \text{m}^2/\text{s}$, which also corresponds to the original fixed value in [2]. Hence, the final VERDICT-AMICO dictionary with an extra un-fixed parameter (d_{EES}) is:

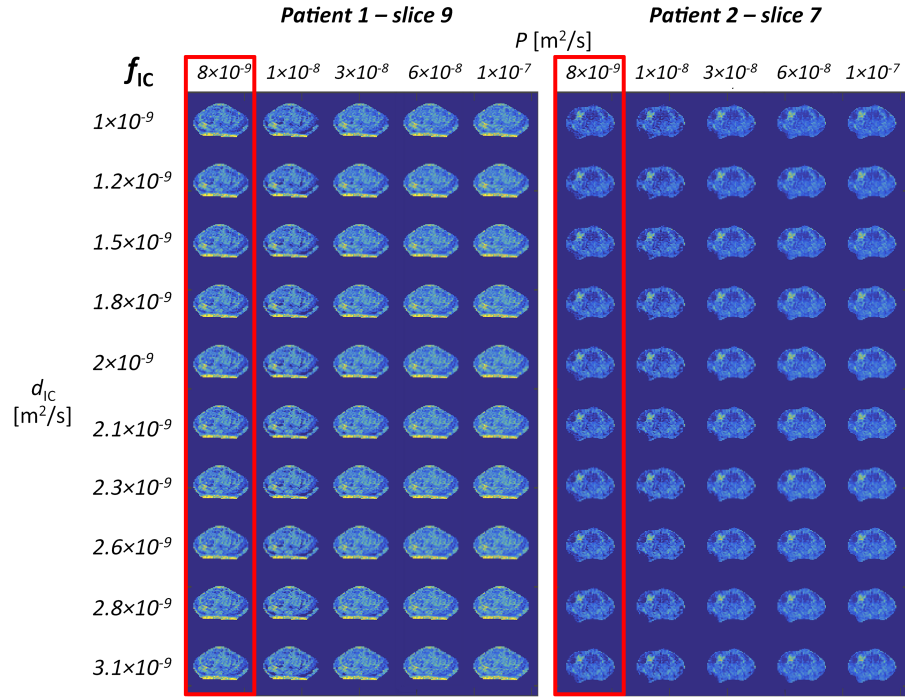


Fig. 2. Qualitative evaluation of VERDICT-AMICO for various fixed $d_{IC} - P$ pairs in two different patients. f_{IC} parametric maps for each $d_{IC} - P$ pair for two different slices from two patients. Each row has the same fixed d_{IC} while each column has a fixed P . The red rectangles indicate which maps correspond to the selected fixed perfusion for different d_{IC} .

- $N_r = 13$ different radii (linearly spaced from 0.01 to 15.1 μm) with fixed $d_{IC} = 2.0 \times 10^{-9} \text{ m}^2/\text{s}$.
- $N_e = 5$ diffusion coefficient for EES: $d_{EES} = 1.1 \times 10^{-9}, 1.6 \times 10^{-9}, 2.1 \times 10^{-9}, 2.6 \times 10^{-9}$ and $3.1 \times 10^{-9} \text{ m}^2/\text{s}$.
- $N_v = 1$, with $P = 8.0 \times 10^{-9} \text{ m}^2/\text{s}$.

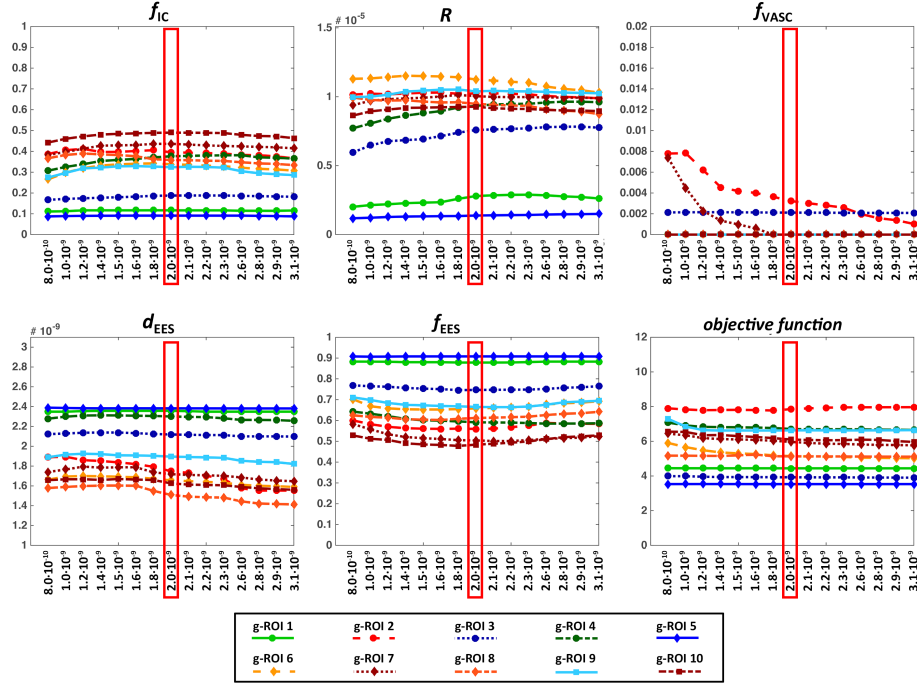


Fig. 3. Parameter performance when changing d_{IC} for fixed $P = 8.0 \times 10^{-9} \text{ m}^2/\text{s}$. The median value for each parameter for all voxels within each of the g-ROIs (represented in different lines) for each d_{IC} value (horizontal axis correspond to the 15 different values for d_{IC}).

3.4 New Parameter estimation

Fig. 4 shows a qualitative comparison for two different patients for the additional maps from VERDICT-AMICO, the (d_{EES}) map and an example of a parametric

combination (f_{IC}/d_{EES}) that increases tumour conspicuity. A standard T2 image part of the mp-MRI evaluation with the ROIs is also shown for anatomical comparison purposes.

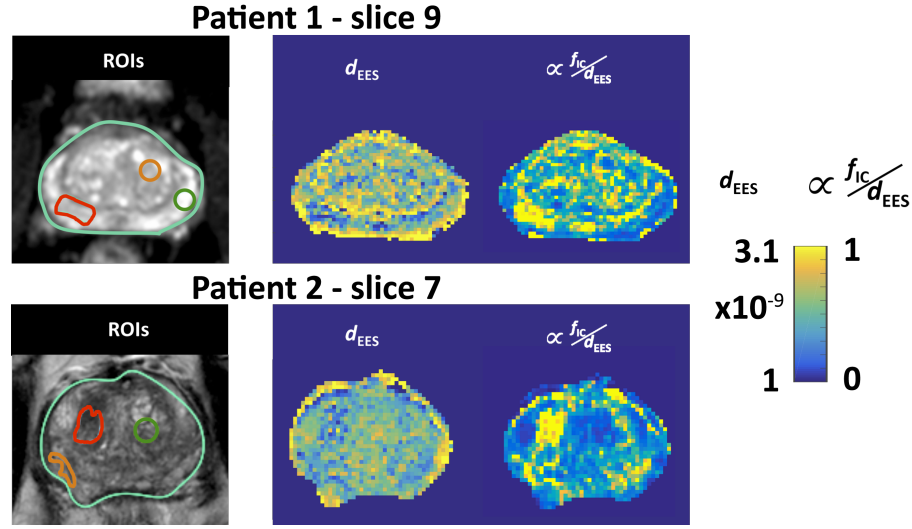


Fig. 4. Qualitative Comparison of new VERDICT-AMICO maps for two different patients. ROIs in T2 image: the whole prostate (light-green-bigger ones). ROI description from left to right: Patient 1, Tumour-PZ (red), suspected-TZ (orange) and Benign-PZ (green). Patient 2, suspected-PZ (orange), Tumour-TZ (red) and Benign-PZ (green).

Fig. 5 illustrates the parameter estimates for all voxels within four of the g-ROIs, normal and Gleason Score 3+4 in TZ and PZ. The new values for the AMICO-VERDICT dictionary compute similar estimates compared with the original fitting for f_{IC} , f_{EES} and R . We note that the vascular volume fraction f_{VASC} is lower for most g-ROIs, showing that unfixing the d_{EES} one of the limitations of VERDICT could be solved. These results are also similar for the individual ROI analysis (not shown).

4 Discussion

We use VERDICT-AMICO to relax the original VERDICT model constraints for prostate cancer characterisation. The improvement in calculation speed that

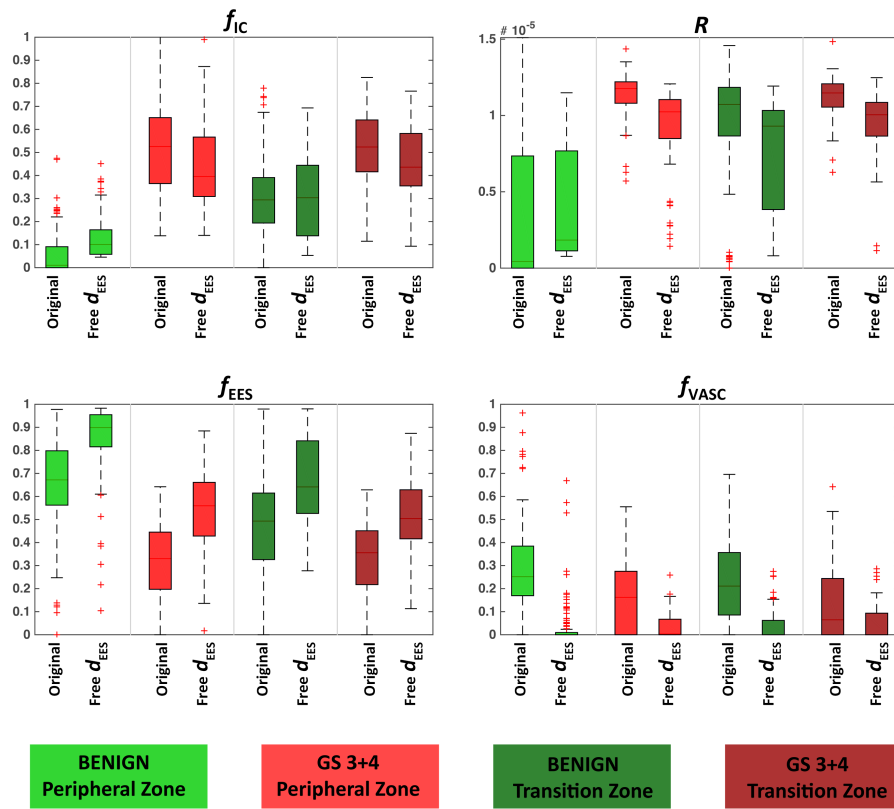


Fig. 5. Parameter estimates comparison for all voxels within four of the g-ROIs using the original VERDICT-AMICO dictionary and the one with unfixed d_{EES} .

AMICO framework offers makes it practical to try different dictionaries for the identification of potentially stable parameter combinations and to help reduce assumptions of fixed compartmental diffusivities that VERDICT studies currently use. We search for dictionary that allows us to reduce the VERDICT parameter constraints and formulate a new version of the model for prostate cancer. Results show that it is possible to eliminate one of the original parameter constraints and unfix the previously fixed d_{EES} parameter allowing for a new diffusivity map.

First we tested the AMICO implementation using the VERDICT prostate model with all the model parameters unfixed. However, this version was unstable as the signal cannot support unambiguous estimation of so many parameters, so we searched for the best constraints to impose. We fix the perfusion parameter to the original value of $P = 8 \times 10^{-9} m^2/s$ and tested the rest of the parameters with a wide range of fixed d_{IC} values to find the best d_{IC} coefficient. We confirmed that different d_{IC} values have small impact on the other parameter estimates with fixed perfusion, as previous studies [13]. Thus, we fixed d_{IC} to the original value for this parameter $d_{IC} = 2 \times 10^{-9} m^2/s$ [2], and obtained the final dictionary. The parameter estimates from the new dictionary are more biophysical plausible and in close agreement with histology (i.e. f_{VASC}). Also, the estimated values for f_{IC} , R or f_{EES} do not hit the boundary constraints after unfixing d_{EES} , which is evidence of improved and stable fitting. To gain sufficient sensitivity for allowing estimation of the full model without constraints would require a much wider sampling of the range of b-values and diffusion times, which is not clinically practical with the existing technology. Currently, the VERDICT DW-MRI acquisition is less than 15 minutes, which is within the time constraints to be used in clinical practice.

The main limitation of the AMICO framework is that the fitting results depend to some extent on the dictionary values, as the regularization has to be set empirically. Graphical Processor Units (GPUs) could also be used to optimise MRI models non-linearly [14] and avoid the dictionary dependency. We used histological information to guide us in the selection of values for our dictionary. However, more samples from larger datasets are required to validate the VERDICT parameters with histology. Finally, the inherent limitations of model-based approaches have to be taken into consideration when interpreting the estimated values. Nevertheless, the results from this study and previous work provide good evidence that this form of the VERDICT prostate model can provide useful information, improving current methods.

To conclude, the AMICO adaptation for VERDICT allowed testing of different values for the previously fixed model parameters in a practical time and helped relax assumptions of fixed compartmental diffusivities that VERDICT currently uses for prostate cancer characterisation.

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